

## RESULTS

- Figure 2 demonstrates the visual assessment of 57 feature maps extracted from one of 46 patients in VAMPIRE Dataset. The upper left panels are the original input CT and corresponding DTPA-SPECT slice. The RefVI scan exhibits defects in both the left upper lobe (LUL) and right upper lobe (RUL). A small number of feature maps successfully detect the defects in both lobes, such as feature #1, 5, 23, 34, 36, 38, 39, 50, and 52. And several other features are only able to detect the major defect that existed in the LUL, which include #10, 14, 18, 26, 30, 31, and 32. Moreover, a few features display high values in the upper lung defect region, see feature #13, 22, 27, 28, 29, 33, 35, 37, 43, 49, 51, and 53, which can be considered as negatively associated with the lung ventilation distribution.
- The box plots in figure 3 show the distributions of voxel-wise Spearman  $\rho$  evaluated between all 57 features and their corresponding RefVI scans (Galligas PET or DTPA-SPECT) for 46 patients. In each box, the central mark indicates the median, and the bottom and top edges indicate the 25th and 75th percentiles, respectively. The whiskers extend to the most extreme data points that not considered as outliers, and the outliers are plotted individually using the “+” symbol. The feature maps are ranked in descending order from left to right based on the median value of  $\rho$ .
- Considering the correlation performance for both Galligas PET and DTPA-SPECT studies, the overall highest correlations archived by feature #30, i.e., *GLRLM-based run length non-uniformity*, with  $0.21 < \rho < 0.65$  (median = 0.45) for Galligas PET study and  $0.29 < \rho < 0.63$  (median = 0.45) for DTPA-SPECT study. The second-highest ranked feature is #1, *l-based Energy*, with  $0.05 < \rho < 0.70$  (median = 0.48) for Galligas PET study and  $0.13 < \rho < 0.74$  (median = 0.43) for DTPA-SPECT study. Moreover, for both studies, the strongest negative correlations come from feature #33, 35, 37, and 51. Specifically,  $\rho$  is approximately in the range [-0.01, -0.70] (median  $\approx$  0.48\$) and [0.09, -0.60] (median  $\approx$  0.30) for Galligas PET study and DTPA-SPECT study, respectively.
- Compared with 37 CTVI algorithms submitted by VAMPIRE Challenge participants [3], the correlation performance of our feature map #1 and #30 exceeds 36 algorithms, and only slightly inferior to No. 20 CTVI algorithm (range: 0.27-0.73, median: 0.49).

This work investigated the association between regional pulmonary function and VBR features maps extracted from the lung computed tomography (CT) images. It is well-known that lung function can be interpreted by the expert based on CT image characteristics (e.g., bronchial thickening, honeycombing) [2]. However, such a phenomenon is typically difficult to measure and quantify. The quantitative VBR approach has the potential to reflect these observations objectively and may serve as a clinical complement to the radiologist ultimately.

## PURPOSE

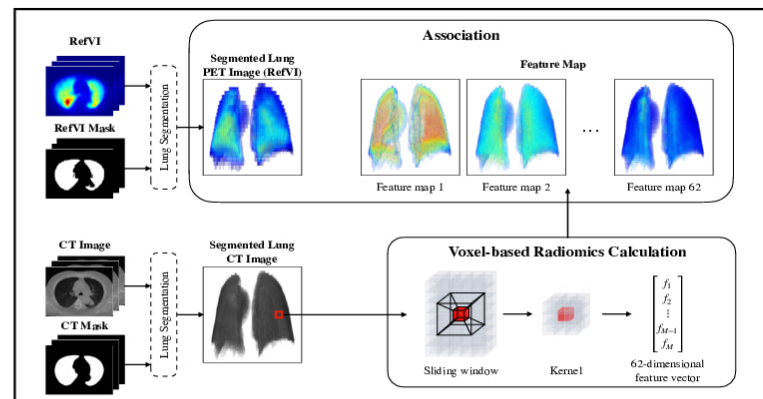
We employed the VBR analysis technique to investigate the potential association of spatially-encoded radiomics features extracted from lung CT images with the pulmonary function measured by ventilation scintigraphy.

## METHOD

- An in-house VBR calculation platform was developed to generalize the conventional image-based radiomics to the voxel level. As in Figure 1, to extract the radiomics features at each voxel, we utilized a 3D sliding window to define a spatial kernel by aligning the voxel of interest with the centre of the window. 57 radiomics features were subsequently calculated within such a rotationally-invariant kernel. By traversing the window over the entire volume, each voxel in the original image can be expressed as a 57-dimensional radiomics feature vector. Consequently, 57 feature maps with the same spatial dimensions as the input image were generated.
- The VBR technique were employed to extracted the feature maps from total of 46 lung CT images in VAMPIRE Galligas PET and DTPA-SPECT Dataset [3]. To test the technique as a potential pulmonary biomarker, we subsequently compared the generated feature maps to corresponding reference ventilation images (RefVIs, e.g., Galligas PET or DTPA-SPECT) as ground truth for pulmonary function based on voxel-wise Spearman coefficients ( $\rho$ ).
- Computed Tomography Ventilation Imaging (CTVI) is another imaging analysis technique that derives regional lung function information from respiratory-correlated CT datasets. In the VAMPIRE Challenge, total of 37 individual CTVI algorithms are submitted by participants and have been evaluated against the corresponding RefVI using Spearman coefficient [3]. Due to similar purposes, same dataset, and the same correlation analysis methods, our results can be directly compared with VAMPIRE CTVI algorithms to assess the overall performance relative to conventional 4DCT-based techniques.

Itemized-based features	1	Energy	25	Short Run Emphasis
	2	Kinergy	26	Short Run Emphasis
	3	Kinergy	27	Long Lead/No. Unleapings
	4	Kinergy	28	Long Lead/No. Unleapings Normalized
Grey-level co-occurrence matrix-based features	5	Area Contrast	29	Long Lead/No. Unleapings
	6	Chen's Proximity	30	Run Length/No. Unleapings
	7	Chen's Proximity	31	Run Length/No. Unleapings
	8	Chen's Proximity	32	Run Length/No. Unleapings
	9	Contrast	33	Run Length/No. Unleapings
	10	Contrast	34	Run Length/No. Unleapings
	11	Contrast	35	Run Length/No. Unleapings
	12	Contrast	36	Run Length/No. Unleapings
	13	Difference Energy	37	Run Length/No. Unleapings
	14	Difference Energy	38	Run Length/No. Unleapings
	15	Energy	39	Run Length/No. Unleapings
	16	Entropy	40	Run Length/No. Unleapings
	17	Histogram-1	41	Run Length/No. Unleapings
	18	Histogram-2	42	Run Length/No. Unleapings
	19	Histogram-3	43	Run Length/No. Unleapings
	20	Histogram-4	44	Run Length/No. Unleapings
Grey-level co-occurrence matrix-based features	21	Info Measures Contrast-1	45	Run Length/No. Unleapings
	22	Info Measures Contrast-2	46	Run Length/No. Unleapings
	23	Info Measures Contrast-3	47	Run Length/No. Unleapings
	24	Info Measures Contrast-4	48	Run Length/No. Unleapings
	25	Info Measures Contrast-5	49	Run Length/No. Unleapings
	26	Info Measures Contrast-6	50	Run Length/No. Unleapings
	27	Info Measures Contrast-7	51	Run Length/No. Unleapings
	28	Info Measures Contrast-8	52	Run Length/No. Unleapings
	29	Info Measures Contrast-9	53	Run Length/No. Unleapings
	30	Info Measures Contrast-10	54	Run Length/No. Unleapings
	31	Info Measures Contrast-11	55	Run Length/No. Unleapings
	32	Info Measures Contrast-12	56	Run Length/No. Unleapings
	33	Info Measures Contrast-13	57	Run Length/No. Unleapings
	34	Info Measures Contrast-14	58	Run Length/No. Unleapings
	35	Info Measures Contrast-15	59	Run Length/No. Unleapings
	36	Info Measures Contrast-16	60	Run Length/No. Unleapings

**Table 1.** All defined 57 radiomics features in our in-house developed voxel-based radiomics calculation platform.



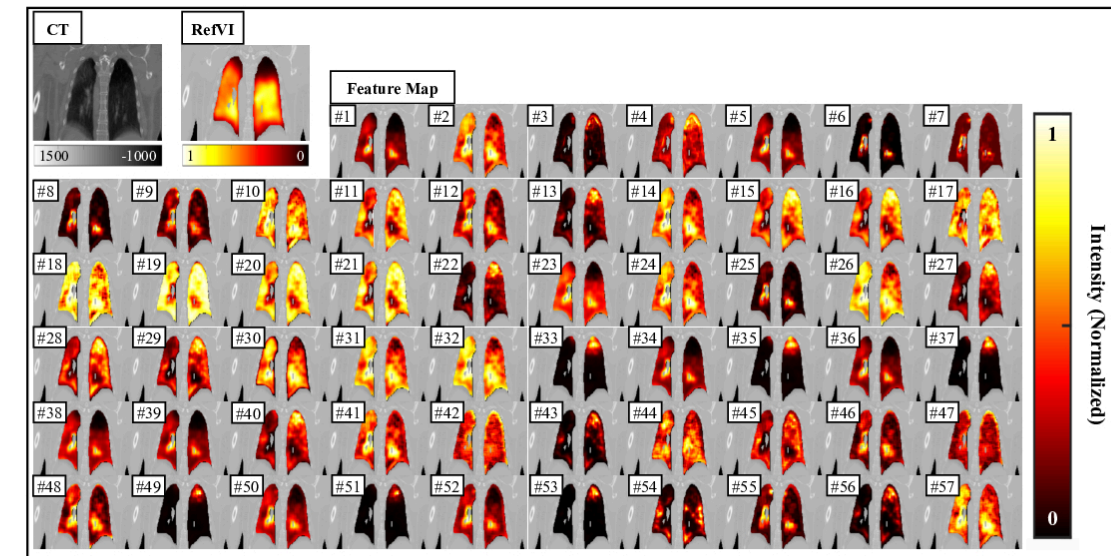
**Figure 1.** The overall workflow of pulmonary voxel-based radiomics feature map extraction.

## DISCUSSION AND CONCLUSIONS

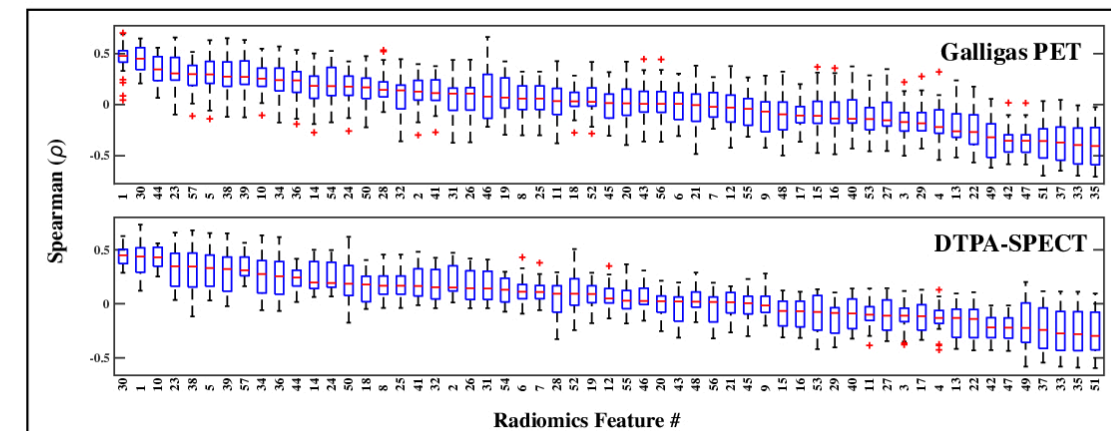
- Quantitative correlation analysis identified that voxel-based radiomics feature maps extracted from lung CT images are partially associated with pulmonary function measured by Galligas PET or DTPA-SPECT ventilation image.
- l*-based energy measures the square of intensity within the image. Higher energy corresponds to denser content. *GLRLM-based run length non-uniformity* assesses the distribution of runs over the run lengths, and a lower value indicates more homogeneity among run lengths in the image. The negatively correlated features #33, 35, 37, and 51 emphasize the low density, heterogeneous coarse structural texture. Collectively, these features together evidence that the homogeneous dense pulmonary CT image often presented as high radiotracer signal, while the regional lung CT content with low density heterogeneous coarse structural texture is often shown as a lack of radiotracer. This results are consistent with the findings based on conventional lung-segmented image-based radiomics analysis by Lafata *et al.* [2]
- Compared with the 4DCT-based CTVI method, the VBR analysis severs as several advantages: (1) the performance of its correlation distribution is better than most VAMPIRE CTVI algorithms; (2) it is easy to implement since the calculations are based on the ready-made and well-defined radiomics features; (3) it only utilizes the time-averaged CT frame instead of 4DCT, which avoids the uncertainty introduced in the deformable image registration (DIR) process.
- This study is just an application of a VBR in lung texture analysis, which is only one aspect of a typical radiomics scope. Besides that, it is reasonable to hypothesize that the VBR technique can be extended to a broader range of applications, such as differentiating benign and cancerous tissue of other body sites, characterizing intratumoral information, assisting prognostic assessment, and combining with the radiogenomic to personalize treatment, etc.

## REFERENCES

- [1] Gillies, Robert J., Paul E. Kinahan, and Hedvig Hricak. "Radiomics: images are more than pictures, they are data." *Radiology* 278.2 (2016): 563-577.
- [2] Lafata, Kyle J., et al. "An exploratory Radiomics Approach to Quantifying pulmonary function in ct images." *Scientific reports* 9.1 (2019): 1-9.
- [3] Kipritidis, John, et al. "The VAMPIRE challenge: A multi-institutional validation study of CT ventilation imaging." *Medical physics* 46.3 (2019): 1198-1217.



**Figure 2.** Visual comparison of ReVfi scans (DTPA-SPECT) and corresponding 57 feature maps generated by voxel-based radiomics technique. The upper left panels are the original input time-averaged CT and corresponding DTPA-SPECT slice. The rest panels are 57 feature maps with feature # indicated in the top left corner. The ReVfi is normalized to [0, 1] and superimposed over the CT at a common coronal slice location for better visualization. Similarly, each feature map is normalized with the same strategy as the ReVfi to provide a similar visual contrast.



**Figure 3.** Spearman correlation ( $\rho$ ) distributions evaluated between each voxel-based radiomics feature maps and the corresponding RefVI. Each box plot represents a specific feature maps # and RefVI modality (Galligas PET or DTPA-SPECT). In each box, the central mark indicates the median, and the bottom and top edges indicate the 25th and 75th percentiles, respectively. The whiskers extend to the most extreme data points not considered outliers, and the outliers are plotted individually using the “+” symbol. The feature maps are ranked in descending order from left to right based on the median value of  $\rho$ .

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