

An Automated Contouring Workflow for Increased Standardization and Efficiency

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INTRODUCTION

AAPM Task Group 263 notes that standard naming benefits the practice of radiation oncology by facilitating communication during routine care and by facilitating data pooling and automatic data extraction and exchange. Consistent naming also benefits automation of downstream tasks, such as automated planning and plan review. The report explores the myriad of challenges of implementing standardized nomenclature, including at the institutional and staff levels. This work explores the approach of using automation, as opposed to staff training, to overcoming some of these challenges.

In addition to non-standardized naming, manual segmentation is time consuming and subject to inter- and intra-observer variability. Recently, technology and training tools have been developed to aid planners with the contouring task, including computer-aided automatic segmentation. Many studies have evaluated the quality of automatic segmentation, and its role in reducing observer variability and reducing contouring time, but its current clinical use is limited. This is partially a result of various challenges in implementing automatically generated contouring tools into a process that involves a range of staffing groups (e.g. physicians, dosimetrists, and physicists), while addressing technical problems and training needs.

AIM

The purpose of this work is to describe and evaluate a new automated contouring workflow, which implements standardized contour naming, coloring, and automatic segmentation. The use of this automation helps address some of the challenges in name and color standardization, and some of the challenges in utilizing computer generated automatic segmentation. Specifically, the automated workflow reduces the training burden of these tools and lessens the dependence of staff adherence to procedures to achieve standardization. Once implemented, standard structure names and colors are automatically provided and a subset of automatically segmented structures are provided by default, allowing planners to use, manually modify, or delete them based on their routine review.

METHOD

The workflow provides standard contour names, colors, and order for each simulation scan. A schematic depiction of the workflow is shown in Figure 1. Contour names are informed by AAPM TG-263 and previous naming practices. A central server automatically applies these contour templates to all simulation scans. Then a subset of the contours is then automatically segmented and sent back to the local server for further planning and approval. During the physics plan check, the final approved contours are returned to the central server to allow for initial contour accuracy scoring with volumetric Dice similarity coefficient and added path length, and for future contour auto-segmentation improvement with machine learning. Finally, planners were surveyed on the usefulness of the initial contours.

RESULTS

In the first nine months of implementation, new workflow managed 511 simulation scans, constituting every simulation done in the department. This included 144 breast, 136 lung, 97 pelvis, 52 head and neck, 45 brain, and 37 abdomen simulations. On these simulations, the workflow generated 12,624 structures, of which 3,137 (~30%) structures were automatically segmented.

When comparing the initial automatically segmented structures to the final approved structures, the mean dice scores were dependent on the structure being segmented, as shown in Table 2. In aggregate, 23% of all automatically segmented structures have a VDSC > 0.99, and 71% have VDSC > 0.7. The mean APL and estimated time saved of each structure is shown in Table 3. Based on the planner surveys, the new workflow saves time on for all treatment sites. The self-reported mean time saved is 24 minutes, while there is not statically significant dependence between treatment sites, due to the small sample size (n = 3)

Brain	Breast/ Chest Wall	H&N	Lung	Pelvis/Female	Pelvis/Male	Abdomen	Extremity
brain	breast	hn	lung	pelvis	pelvis	abdo	ext
Body	Body	Body	Body	Bladder	Bladder	Body	Body
Bolus_xxmm	Bolus_xxmm	Bolus_xxmm	Bolus_xxmm	Body	Body	Bolus_xxmm	Bolus_xxmm
Bones	Bones	Bones	Bones	Bolus_xxmm	Bolus_xxmm	Bones	Bones
Brain	Heart	Brain	BrachPlex L	Bone Marrow	Bone Marrow	Bowel Large	
Brain-PTV	LN Ax L1 L	Brainstem	BrachPlex R	Bones	Bones	Bowel Small	GTV
Brainstem	LN Ax L1 R	Brainstem	Bronchial Tree L	Bowel Large	Bowel Large	Bowel Space	CTV
		3PRV					
Brainstem 3PRV	LN Ax L2 L	Cochlea L	Bronchial Tree R	Bowel Small	Bowel Small	Esophagus	PTV
Cochlea L	LN Ax L2 R	Cochlea R	Carina	Bowel Space	Bowel Space	Heart	
Cochlea R	LN Ax L3 L	Esophagus	Chest Wall L	Genitalia Ext	Genitalia Ext	Kidney L	
Eye L	LN Ax L3 R	Larynx	Chest Wall R	Rectum	Penile Bulb	Kidney R	
Eye R	LN IMN L	Lips	Esophagus	SacraIPlex	Prostate	Liver	
Lens L	LN IMN R	Mandible	Great Ves	Rectum	Spinal Cord		
Lens R	LN Supraclav L	Oral Cavity	Heart	GTV	SacraIPlex	Spinal Cord	SPRV
Opt Chiasm 3PRV	LN Supraclav R	Parotid L	Lung Bilat	CTV	SeminalVes	Stomach	
Opt Chiasm	Lung Bilat	Parotid R	Skin	PTV			
Opt Nrv L	Nipple L	Spinal Cord	Spinal Cord		GTV	GTV	
Opt Nrv L 3PRV	Nipple R	Spinal Cord	Spinal Cord		CTV	CTV	
		SPRV	SPRV				
Opt Nrv R	Scar	Submandibul ar L			PTV	ITV	
		ar R					
Opt Nrv R 3PRV	Spinal Cord	Submandibul ar R	GTV			PTV	
Spinal Cord	Spinal Cord SPRV		CTV				
Spinal Cord SPRV		GTV	ITV				
		GTV	CTV	PTV			
GTV	CTV	PTV					
CTV	PTV						
PTV							

Table 1: The seven anatomical treatment sites (with pelvis sub-divided between male and female), their DICOM tags, and the automatically generated contour list. The automatically generated structures were chosen by planners and physicians in an estimated > 5% of plans in that region.

Contour	Dice score > 0.99	Dice score > 0.7	Dice score < 0.7
Lung, Left	86%	100%	0%
Lung, Right	79%	100%	0%
Bladder	40%	93%	7%
Seminal Vesicles	40%	80%	20%
Femur, Right	39%	83%	17%
Femur, Left	35%	88%	12%
Spinal Cord	25%	46%	54%
Rectum	20%	100%	0%
Eye, Left	17%	61%	39%
Eye, Right	17%	44%	56%
Esophagus	15%	50%	50%
Brainstem	14%	64%	36%
Parotid, Right	11%	78%	22%
Optic Chiasm	11%	44%	56%
Heart	5%	97%	3%
Prostate	0%	100%	0%
Mandible	0%	100%	0%
Parotid, Left	0%	75%	25%
Oral Cavity	0%	33%	67%
Optic Nerve, Left	0%	38%	63%
Optic Nerve, Right	0%	57%	43%

Table 2: The percent of automatically segmented structures that have a dice score of greater than 0.99, 0.9, and 0.7 when compared with the final approved structures. These represent contours that of decreasing usefulness to planners.

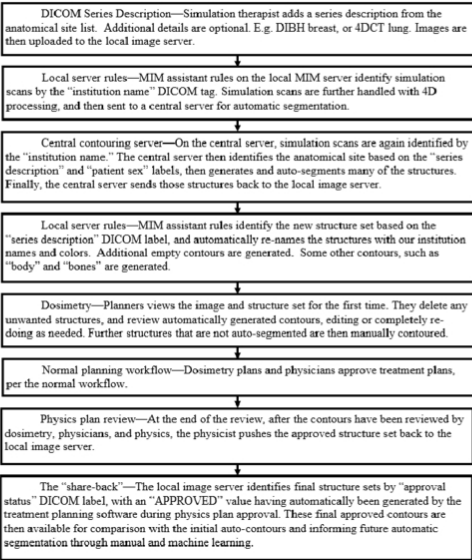


Figure 1: The schematic of the new automated workflow. The workflow is initiated at the time of initial CT-simulation, when the simulation therapist assigns a DICOM tag to each scan in the "series description" label, describing the scan as one of seven pre-determined anatomical treatment sites

CONCLUSIONS

The implementation of the new workflow has two principle benefits. First is the increased standardization of contour name, color, and order, which anecdotally improves routine patient care. Physicians and planners note fewer instances of contours being forgotten and easier plan review, as OAR and target volume dose constraints are examined quickly with predictable structure color and order. And the second benefit is reduced contouring time. Both methods of evaluating the effect of implementing the new workflow show some amount of time saving.

In order to utilize the new workflow, some training efforts are required. Specifically, simulation therapists need to be trained to label simulation scans with the correct DICOM tag identifying the treatment site, and planners need to be trained to delete and restart a structure, and not attempt to modify it, if the initial structure is considerably incorrect.

Future work will automate some contouring work done after structures have been reviewed. The expansion of OARs into planning organ at risk volumes (PRV) and the creation of planning pseudo-structures can be similarly automated. Additionally, the standardization of names and automatic segmentation allows for easier and potentially fully automatic planning with knowledge-based planning.

This workflow is scalable to radiation treatment centers of any size. Aside from increased structure standardization, this process has been demonstrated to reduce planner contouring time with automatic segmentation that provides time saving initial structures to planners. Finally, this automated contouring workflow can be implemented without major re-training of therapists and treatment planners.

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