

Patient-Specific QA for External Beam Radiotherapy Using the HYPERSCINT Plastic Scintillation Detector

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INTRODUCTION

Plastic scintillation detectors (PSDs) have interesting dosimetric properties, including small size and energy independence. These advantages make them well suited for VMAT patient-specific QA, either alone or in conjunction with a detector matrix.

AIM

This work aims to determine if the HYPERSCINT scintillation dosimetry research platform (Medscint inc., Quebec City, Canada) can replace the classic ion chamber in a clinical patient-specific QA workflow.

METHOD

A custom-made, 3D-printed detector holder for the Delta4 Phantom+ diode matrix (Scandidos, Uppsala, Sweden) was designed to house both a A1SL ionization chamber (Standard Imaging, Middleton, WI) and a HYPERSCINT PSD probe (Fig. 1). The center of the chamber and PSD was placed on the same transverse plane, at a center-to-center distance of 6.5 mm from one another. The insert was 3D printed in PLA using an S5 3D printer (Ultimaker, Utrecht, Netherlands) and matches the density of the acrylic contained in the Delta4 Phantom+.

A total of 36 prostate plans (without pelvic nodes) and 47 palliative plans were selected for the study. Plans were delivered on the Phantom+ using a VersaHD linear accelerator (Elekta)(Fig 2) and measured simultaneously on both detectors. Difference between planned and measured dose (corrected for daily linac output) were computed for both the chamber and the PSD and the results from both detectors were compared for consistency.

RESULTS

As seen in Fig. 3, differences between VMAT planned and measured dose for both detectors are within 1.5% of the planned values, as expected from simple cases such as prostate and palliative sites. Dose difference between the measured and planned dose for the ionization chamber was $(0.3 \pm 0.2)\%$ (average ± 1 standard deviation) for the prostate cases and $(0.0 \pm 0.5)\%$ for the palliative cases. For the HYPERSCINT alone these values stand as $(0.9 \pm 0.3)\%$ for the prostate cases and $(0.5 \pm 0.7)\%$ for the palliative cases.

A 0.5% offset on average between the HYPERSCINT and the ionization chamber can be seen from the measurements, as shown in Fig. 4. When comparing pairs of measurements (ion chamber vs PSD), the PSD overestimated the ion chamber dose by $(0.6 \pm 0.2)\%$ for the prostates cases and $(0.5 \pm 0.4)\%$ for the palliative cases. The source of this offset is still to be investigated, but are nevertheless deemed small enough to judge the HYPERSCINT a valid candidate to replace the chamber in future QA measurements using this setup.

Figure 3: Difference between QA planned dose and measured dose, for both detectors under investigation. Deviations typically range from -1.5% to 1.5% for both detectors.

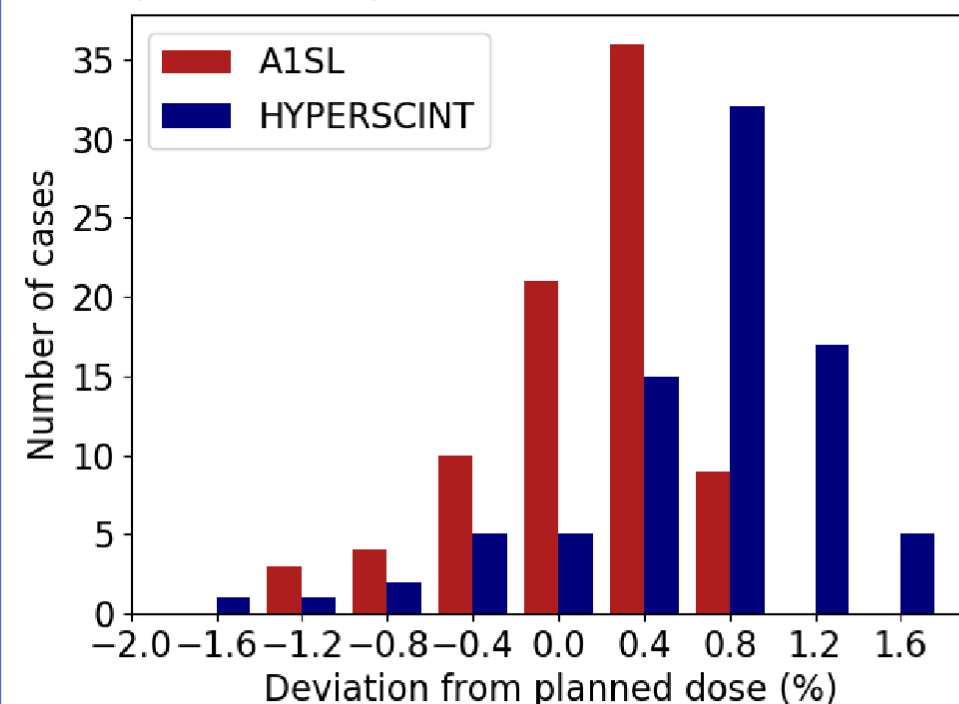


Figure 1: Sectional view of the custom-made insert for the Delta4 Phantom+.

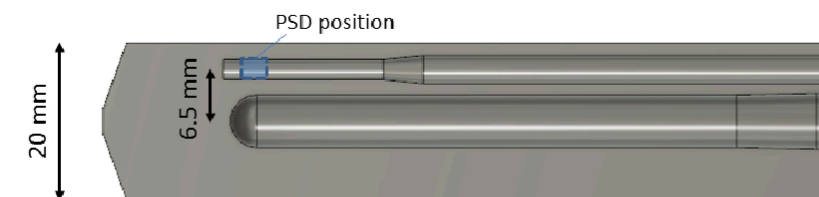


Figure 2: Delta4 measurement setup at the linear accelerator.

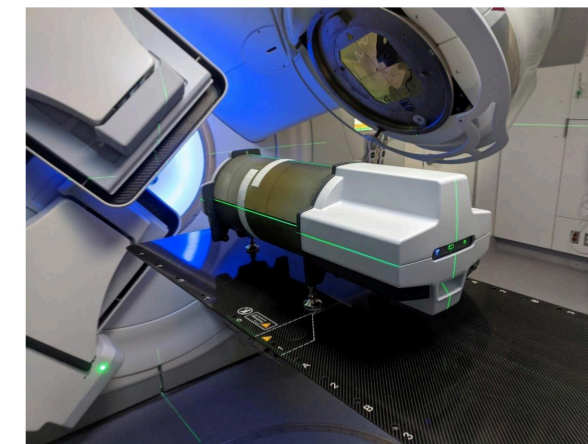
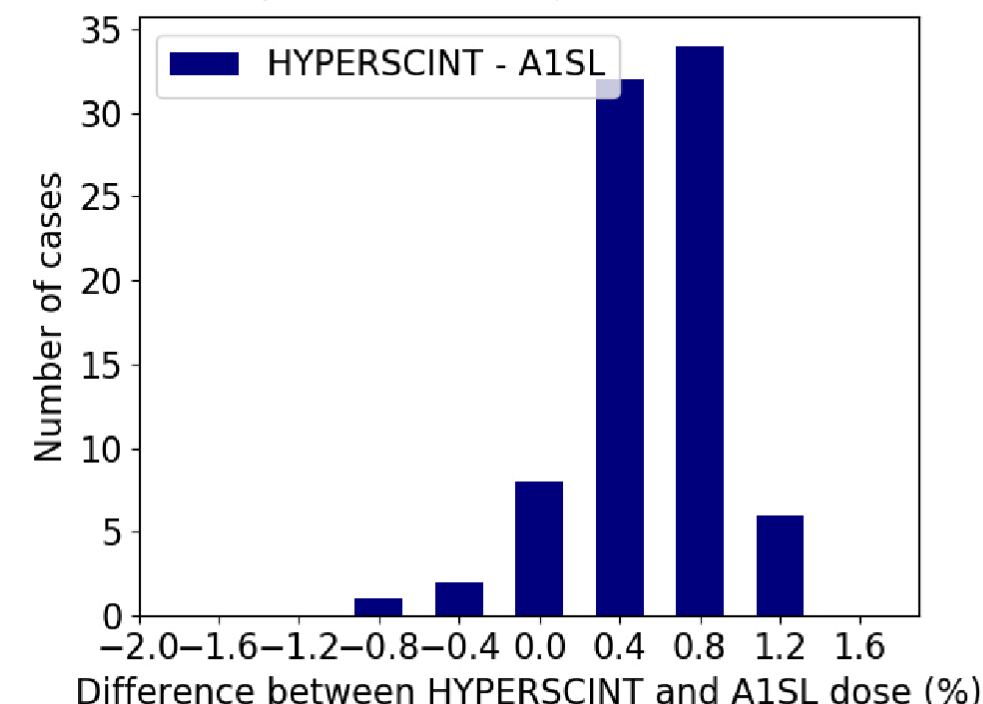


Figure 4: Difference between HYPERSCINT and A1SL measured dose difference. On average a 0.5% overestimate in dose is observed for the HYPERSCINT compared to the A1SL.



CONCLUSIONS

Albeit a systematic offset of about 0.5% between the ion chamber and the PSD measured doses, the HYPERSCINT plastic scintillation dosimetry research platform shows enough accuracy to be used as a surrogate for an ion chamber in the measurement of VMAT patient-specific QA plans.

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See also : poster #PO-GeP-T-161, HDR Brachytherapy Technique Commissioning Using the HYPERSCINT Plastic Scintillation Detector

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