

# SIMULATION-BASED ANALYSIS OF DOSIMETRIC UNCERTAINTY DUE TO CATHETER RECONSTRUCTION ERROR IN TRUS-GUIDED PROSTATE HDR BRACHYTHERAPY

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## BACKGROUND

Geometric error in catheter reconstruction impacts target coverage and OAR sparing in brachytherapy

## STUDY AIM

To assess robustness of our HDR prostate procedure *via* simulation of errors and re-calculation of target and OAR dose

## METHODS

### Fast Dose Calculation

- TG-43U1 implemented in NVIDIA CUDA-C for rapid parallel execution ( $\sim 25\times$  speedup vs. CPU)
- Validated by comparison to clinical treatment planning system (Oncentra Brachy)

### Patient Cases

- 31 TRUS-guided HDR prostate single fraction boost cases (prescription dose = 1500 cGy) anonymized
- Dose recalculated under simulated catheter errors (systematic and random errors)
- DVH curves / GEC-ESTRO key metrics recorded

### Ultrasound-derived catheter error estimates

- Catheter profiles (axial and lateral) measured on US
- FWHM used to define a spatially-varying Gaussian error distribution to sample (Figure 1)

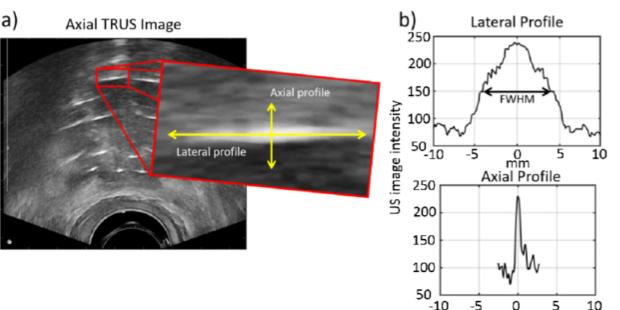


Figure 1: a) US image of prostate with implanted catheters.  
b) Lateral and axial profiles measured from ultrasound.

## RESULTS - SYSTEMATIC SHIFTS

- Systematic shifts of [1-5 mm] applied to all catheters in ANT/POST, LEFT/RIGHT, and SUP/INF directions, simulating mis-calibration or misalignment of equipment
- GEC-ESTRO DVH reporting parameters calculated for each simulated shift

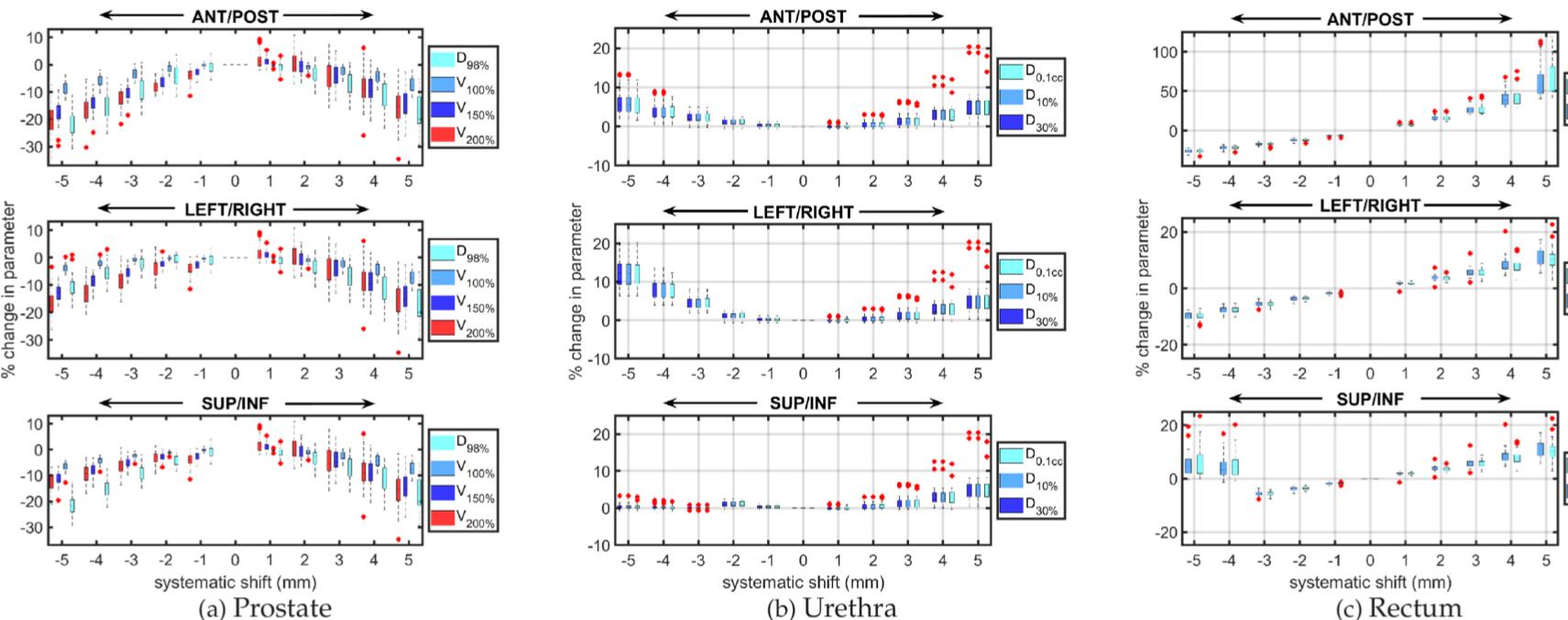


Figure 2: Change in GEC-ESTRO DVH parameters (for all cases) for (a) prostate, (b) urethra, and (c) rectum as a function of introduced systematic errors. Boxplots show the mean and interquartile range, while red dots show outlying cases.

- Systematic errors of  $\leq 2$  mm result in  $\leq 2\%$  change in target  $V_{100\%}$ ,  $\leq 5\%$  change in  $D_{98\%}$  and acceptable urethra dose variability
- Rectal dose criteria very sensitive to posterior shifts - validates conservative rectal dose limits in planning

## CONCLUSIONS

- Systematic errors of less than 2 mm result in less than 2% change in target  $V_{100\%}$  and less than 5% drop in  $D_{98\%}$
- Conservative image-derived random errors result in small changes in prostate  $V_{100\%}$  and  $V_{125\%}$ , but significant change in  $D_{98\%}$
- OAR dose criteria relatively unaffected by random errors
- Rectal dose impacted by systematic ANT/POST shifts
- QA tolerances of 2 mm are reasonable, and implant and planning strategy is robust against random geometric errors
- Developed software will be useful in evaluation of automatic catheter segmentation methods

## REFERENCES

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## CONTACT INFORMATION

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## RESULTS - RANDOM ERRORS

- Image-derived Gaussian error distributions in probe axial and lateral directions sampled via Monte Carlo technique
- Dose and DVH parameters recalculated for 1000 iterations per case (sample shown in Figure 3)
- Parameters are compared for the prostate, CTV (prostate + margin), urethra, and rectum

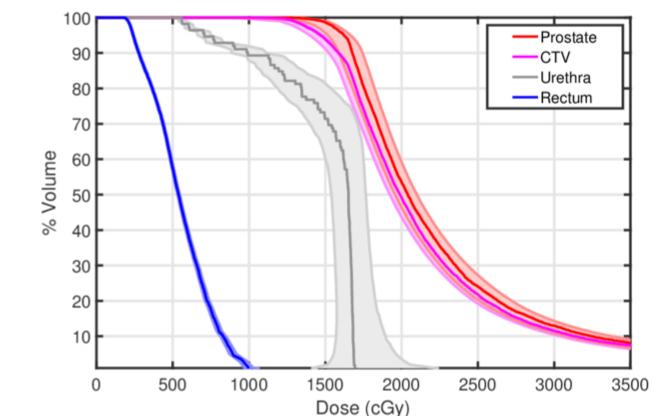


Figure 3: Confidence-interval DVH curves for a single case. The solid line denotes the clinical plan, while the shaded region indicates the 95% confidence interval from Monte Carlo simulations.

- Small mean changes to  $V_{100\%}$  for targets, larger changes in  $D_{98\%}$
- Very small changes in OAR DVH parameters

Structure	Parameter	Mean % Change
Prostate	$D_{98\%}$	$-7.0 \pm 2.4$
	$V_{100\%}$	$-0.6 \pm 0.9$
	$V_{125\%}$	$-1.7 \pm 6.2$
CTV	$D_{98\%}$	$-12.5 \pm 1.6$
	$V_{100\%}$	$-1.1 \pm 0.9$
	$V_{125\%}$	$-8.8 \pm 4.2$
Urethra	$D_{0.1cc}$	$+1.6 \pm 3.7$
	$D_{2cc}$	$-0.1 \pm 1.1$

Table 1: Mean and standard deviation of difference, in percent, of GEC-ESTRO reporting parameters relative to clinical plans.

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